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# A novel tool for quantitative measurement of distortion in keratoconus

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1	A novel tool for quantitative measurement of distortion in keratoconus
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11	
12	Abstract
13	Background: Keratoconus is associated with thinning and anterior protrusion of the cornea resulting
14	in the symptoms of blurry and distorted vision. The commonly used clinical vision tests such as visual
15	acuity and contrast sensitivity may not reflect the symptoms experienced in keratoconus and there are
16	no quantitative tools to measure visual distortion. In this study, we used a quantitative test based on
17	vernier alignment and field matching techniques to quantify visual distortion in keratoconus and
18	assess its relation to corneal structural changes.
19	Methods: A total of 50 participants (25 keratoconus and 25 visually normal) completed the
20	experiment where they aligned supra-threshold white target circles in opposite field in reference to
21	guide lines and circles to complete a square structure. The task was repeated five times and the global
22	distortion index (GDI) and global uncertainty index (GUI) were calculated as the mean and standard
23	deviation respectively of local perceived misalignment of target circles over five trials.
24	<b>Results:</b> Both GDI and GUI were higher in participants with keratoconus compared to controls ( $p <$
25	0.01). Both parameters correlated with the best corrected visual acuity, maximum corneal curvature
26	(K <sub>max</sub> ), topographical keratoconus classification (TKC) and central corneal thickness (CCT).
27	<b>Conclusion:</b> Our findings show that the quantitative measure of distortion could be a useful tool for
28	behavioural assessment of progressive keratoconus.

#### 29 Introduction

30 Keratoconus is a progressive corneal condition characterised by anterior protrusion and thinning of 31 the cornea. The aetiology of the condition is multifactorial with recent studies suggesting a role of 32 inflammatory mechanisms.(1, 2) The estimated prevalence of keratoconus is reported to be 1 in 84 (3) to 1 in 375 (4) in young adults. The condition has a genetic heterogeneity and involves both 33 34 autosomal dominant and autosomal recessive patterns.(5) The corneal structural changes lead to 35 irregular astigmatism and myopia with the symptoms of blurry vision, increased sensitivity to glare, 36 and distorted vision due to higher order aberrations.(6-8) The symptoms begin in adolescence or early 37 adulthood and usually slowly progresses until mid-adulthood.(8) 38 39 The commonly assessed structural measurements in keratoconus include corneal curvature, corneal

40 topography, and corneal thickness using keratometer, corneal topographer, and ocular coherence 41 tomogram (OCT) respectively. Visual acuity is the most commonly measured visual function 42 outcome in the clinical setup. However, visual acuity is not a good predictor of symptoms experienced 43 in keratoconus and vision related quality of life is reduced even in early stages of the disorder while 44 good visual acuity may be maintained. (9-12) Contrast sensitivity meanwhile correlates both with 45 higher order aberration (7, 13) and topographic indices (14). However, clinically available contrast 46 sensitivity charts may not be appropriate for the evaluation of moderate to advanced keratoconus. (15) 47 Hence there is a lack of a perceptual visual measure that reflects symptoms experienced in 48 keratoconus. Different parameters indicate keratoconus progression, and therefore need for 49 intervention with methods such as collagen cross-linking. These include an increase in maximum 50 corneal curvature by 1 D over a year (16), increase in astigmatism by 1 - 3 DC over 6 months, and 51 reduction in central corneal thickness by 5% over 6 months (17). Previous studies have demonstrated 52 variable correlation of best-corrected visual acuity with these parameters, with contrast sensitivity 53 again showing a better correlation.(18, 19) However, monitoring clinical progression requires 54 specialist imaging equipment, and therefore regular visits to an eye care professional are required. 55 Recently a new scoring system that includes clinical measures and the patient characteristics such as 56 patient reported quality of vision, the Dutch Crosslinking for Keratoconus Score, is reported to be

57 better at predicting when medical intervention may be needed.(20) A reliable perceptual

58 measurement that better reflects patient's visual status may further aid development of such scoring

- 59 system. Such a measure could also potentially be used as a home-based test.
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00	
61	While visual distortion is one of the most common symptoms in keratoconus, there are currently
62	limited methods to quantify such distortion and none as far as we are aware specifically designed for
63	keratoconus. There have been approaches to quantify distortion using hyperacuity tasks in different
64	ocular conditions. (21-24) Hyperacuity refers to the visual system's ability to perform spatial tasks
65	beyond the eye's classical resolution limit with thresholds as low as 3 to 6 secs of arc. (25, 26) Vernier
66	alignment (vernier acuity), a classic hyperacuity task where participants discriminate difference in the
67	relative spatial localisation of two or more visual stimuli such as lines or dots has been used in
68	previous studies (27-29). The use of such methods for conditions such as amblyopia (30) and age-
69	related macular degeneration (AMD) (31) have demonstrated perceptual distortions exhibit a similar
70	dissociation from visual acuity as clinical keratoconus indices. Thus, evaluating perceptual distortions
71	may provide a more nuanced characterisation of visual function for ocular diseases.
72	
73	In this study, we used a quantitative paradigm based on both vernier alignment and field matching
74	techniques to quantify visual distortion experienced in keratoconus and assess its relation to corneal
75	structural changes. Providing a means to reliably and systematically characterise the visual deficit in
76	keratoconus enables future studies exploring the impact of established treatments upon these deficits.
77	
78	Methods
79	Participants:
80	A total of 25 participants (mean age = $29.84 \pm 7.46$ years, 15 females) with keratoconus at different
81	disease stages and 25 normal controls (mean age = $22.12 \pm 2.62$ years, 17 females) were recruited for
82	the study. All participants underwent measurements of the best-corrected monocular visual acuity

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(BCVA) with Bailey-Lovie log MAR chart after refraction with autorefractor (Topcon KR-8000PA)

84	by an optometrist. The corneal assessment to ascertain keratoconus signs was carried out using
85	Haag-Streit slit-lamp biomicroscope. The corneal mapping was conducted using a corneal
86	topographer (Oculus Keratograph D-35582) and the central corneal thickness (CCT) was measured
87	using anterior segment ocular coherence tomogram (Topcon 3D OCT-2000). A specialist
88	established the keratoconus diagnosis based on the maximum corneal curvature (K <sub>max</sub> ) of $\geq$ 50.00Ds
89	with topographic keratoconus classification (TKC) grading of >1.0 and the presence of classical
90	keratoconus sign in either eye. The signs considered were Munson's sign, Rizutii's sign, Vogt striae,
91	and Fleischer ring, in addition to scissors reflex on retinoscopy. The clinical details of the keratoconus
92	and control group are presented in Table 1.

# 94 Table 1: Clinical attributes of keratoconus and control participants

Clinical parameters	Keratoconus ( $n = 50$ eyes)	Control ( $n = 50$ eyes)
Best-corrected visual acuity, log MAR, mean (SD), mean	0.21 (0.27), 6/9.6	-0.09 (0.06), 6/4.8
Snellen		
Refractive error (Sphere), diopter cylinder, mean (SD)	- 2.52 (2.85)	- 1.14 (1.61)
Refractive error (Cylindrical), diopter cylinder, mean (SD)	-3.45 (2.10)	-0.77 (0.90)
Maximum corneal curvature, dioptre, mean (SD)	54.48 (6.09)	45.66 (1.58)
Mean corneal curvature, dioptre, mean (SD)	47.03 (3.96)	44.51 (1.41)
Central corneal thickness, micrometre ( $\mu$ m), mean (SD)	495.34 (47.50)	554.36 (25.71)

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## 96 Stimuli and procedure

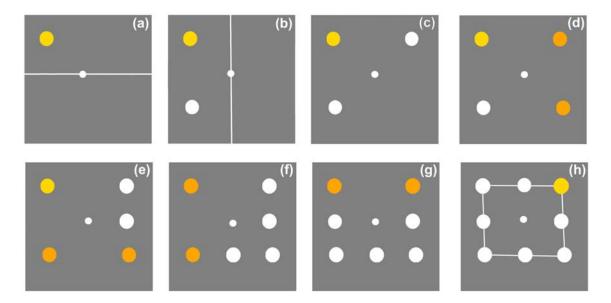
97 The experimental stimulus was created and presented using MATLAB (32) software with

98 psycholbox extensions (Psycholbox 3.0) (33, 34) and presented on a computer screen with the

99 resolution of 1920 x 1080 pixels. The task combined vernier alignment and field matching techniques.

- 100 The stimuli consisted of eight circles (suprathreshold acuity and contrast) each subtending 0.37° at the
- 101 viewing distance of 90cm. The task for the observer was to align target circles with computer mouse
- 102 click in relation to a reference line and circles presented against a 75% contrast grey background
- 103 monocularly. At the start of the experiment a white central fixation circle  $(0.14^\circ)$  and a white
- 104 horizontal line were presented. This was followed by the presentation of a yellow reference circle

105  $(0.37^{\circ})$  at the eccentricity of  $0.73^{\circ}$  from the central fixation (Figure 1; a). The task for the participant 106 was to align a white target circle with the yellow reference circle at an equal distance from the 107 horizontal reference line (Figure 1; a & b). After the placement of the first circle, the reference line 108 was presented vertically, and the participant aligned the next target circle in the opposite field (Figure 109 1; b & c). Following this, the reference line was removed, and the participant placed another target 110 circle to complete the remaining corner of a "virtual square" (Figure 1, d). Following this, two dots 111 changed colour to orange (reference dots) and the task for the participant was to place the target 112 circles at the mid-point and in alignment with these reference dots (Figure 1, e - g). The process 113 continued until a square shape was completed by placing a total of seven target circles. (Figure 1, h). 114 Participants fixated on a central target  $(0.14^{\circ})$  throughout the task. There was no time limit for the 115 completion of the task. If the participant reported having made an error with the dot placement (e.g. 116 mis-click), the researcher removed the dot to allow another attempt.



117

#### 118 Figure 1: Schematic representation of the experimental task. The task was to position a supra-threshold contrast

## 119 white circle in relation to the white line and/or yellow/orange circles to complete a square shape (bottom right panel).

- a) Starting view for the participant (starting corner is randomised). Participant aligns a white dot (shown in b) with yellow
- 121 dot on the opposite side of the white line to match the reference space.
- b) Repeat of a) using vertical reference line and horizontal reference space.
- 123 c d) Complete the square by aligning the remaining dots horizontally and vertically.
- e) Fill in the space between the two orange dots in alignment with the central fixation target.

125 f - g) Repeat step e) on each side to finish reconstructing the square.

126 h) Final image shown to the participant after all clicks are completed.

127 Written informed consent was obtained from all participants once the nature of the experiment was 128 explained. The experiment was completed monocularly with the patient's best correction in place in a 129 dark room, with the computer monitor being the only light source. The distance from the monitor was 130 controlled using head and chin rest. The task was repeated five times and the global distortion index 131 (GDI) and global uncertainty index (GUI) were calculated as the mean and standard deviation 132 respectively of local perceived misalignment of target circles over five trials. (30) The distortion data 133 for both keratoconus and normal controls did not follow a normal distribution (Shapiro-Wilk test, p < p134 0.001) hence nonparametric statistics were used for all analyses. The study followed the tenets of 135 Helsinki declaration on human research participants and the research protocol was approved by the 136 Campus Research Ethics Committee of the Faculty of Health, St. Augustine campus, the University of 137 the West Indies.

138

# 139 Results

The visual distortion measured as the global distortion index (GDI) was higher in keratoconus eyes (n = 50, median (M) = 0.43°) compared to the control eyes (n = 50, M = 0.29°), Mann-Whitney U = 756, 142 z = -3.41, p = 0.001. Similarly, the global uncertainty index (GUI) was also higher in keratoconus 143 eyes (n = 50, M = 0.39°) compared to the control eyes (n = 50, M = 0.25°), Mann-Whitney U = 763, z

144 = -3.36, p = 0.001. (Figure 2)

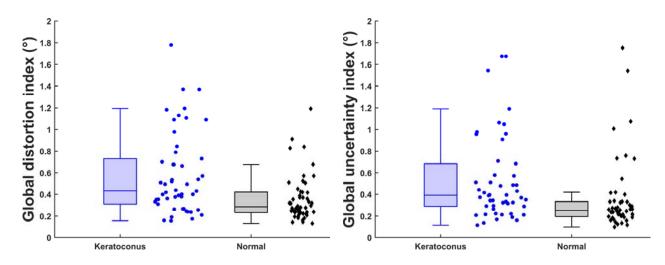




Figure 2: Boxplots comparing global distortion index (left panel) and global uncertainty index (right panel) between
keratoconus eyes (n = 50) and normal eyes (n = 50). Box bounds: upper/lower quartile; horizontal bar within box
bounds: median. All data points are also presented.

151 The relation between clinical parameters and distortion indices (GDI and GUI) were investigated 152 using Spearman's rank order correlation. These are shown for GDI in Figure 3 and GUI in Figure 4 153 for BCVA (Figure 3a, 4a), maximum corneal curvature (Figure 3b, 4b), central corneal thickness 154 (Figure 3c, 4c) and topographic keratoconus classification (TKC) scores (Figure 3d, 4d). Among the 155 clinical parameters, BCVA strongly correlated with maximum corneal curvature (Spearman's rho ( $\rho$ ) 156 = 0.73, p < 0.001) and moderately correlated with TKC scores ( $\rho = 0.49, p < 0.001$ ) but not with 157 central corneal thickness ( $\rho = -0.27$ , p = 0.06). Thus, poorer BCVA was associated with greater 158 maximum corneal curvature and TKC scores. 159 160 For the distortion indices, GDI was weakly correlated with BCVA ( $\rho$ ) = 0.39, p = 0.005, Figure 3a), moderately correlated with maximum corneal curvature ( $\rho = 0.55$ , p < 0.001, Figure 3b) and weakly 161 162 correlated with TKC scores ( $\rho = 0.32$ , p = 0.02, Figure 3d). A moderate negative correlation was also

- 163 observed between GDI and central corneal thickness ( $\rho = -0.43$ , p = 0.002, Figure 3c). Thus, higher
- GDI was associated with poorer BCVA, greater maximum corneal curvature and TKC scores, andlower central corneal thickness.
  - 7

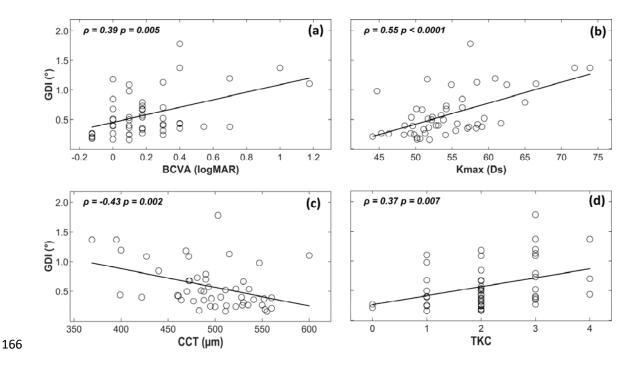




Figure 3: The scatterplots showing correlation between global distortion index (GDI) with a) the best corrected visual
acuity (BCVA), b) maximum corneal curvature (K<sub>max</sub>), c) central corneal thickness (CCT), and d) topographic
keratoconus classification (TKC). The red line represents least square regression line. The Spearman's rho (ρ) and
the *p* value are also provided.

173 The global uncertainty index (GUI) also exhibited a weak positive correlation with BCVA ( $\rho = 0.35$ ,

174 p = 0.01, Figure 4a), moderate correlation with maximum corneal curvature ( $\rho = 0.53$ , p < 0.001,

Figure 4b) and weak correlation with TKC scores ( $\rho = 0.32$ , p = 0.02, Figure 4d). A moderate

176 negative correlation was also observed between the GUI and the central corneal thickness (CCT) ( $\rho =$ 

177 -0.44, p = 0.001, Figure 4c). Thus, higher GUI was associated with poorer BCVA, greater maximum

178 corneal curvature and TKC scores, and lower central corneal thickness.

179

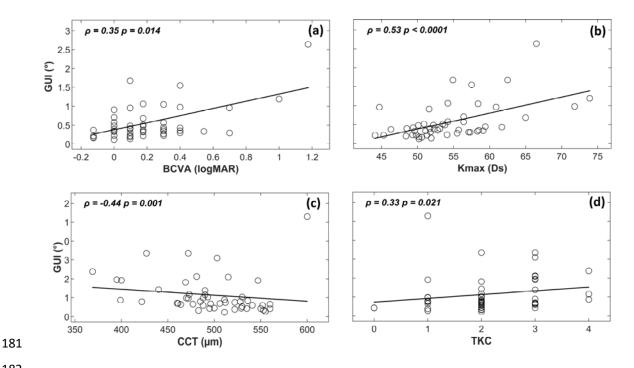




Figure 4: The scatterplots showing correlation between global uncertainty index (GUI) with a) the best-corrected visual acuity (BCVA), b) maximum corneal curvature ( $K_{max}$ ), c) central corneal thickness (CCT), and d) topographic keratoconus classification (TKC). The red line represents least square regression line. The Spearman's rho ( $\rho$ ) and the p value are also provided.

#### 188 Discussion

189 This study for the first time quantitatively evaluated visual distortion experienced in keratoconus. The

190 results showed that visual distortion was higher in individuals with keratoconus compared to the

191 normally sighted controls. The distortion indices also correlated with commonly measured clinical

192 metrics of keratoconus such as  $K_{max}$  and TKC.

193

194 The results demonstrate that measurements of visual distortion obtained with our paradigm

- 195 differentiate individuals with keratoconus from those without. A similar paradigm based on vernier
- alignment has been used to measure perceptual distortion in amblyopia and AMD before. (30, 31, 35,
- 197 36) However these tests are lengthy to conduct in a clinical setting compared to the combined vernier
- 198 alignment and field matching task used in the current study, which takes just a few minutes to

complete. This renders our paradigm a more viable option for characterising visual distortionsassociated with keratoconus in clinical settings.

201

202	Both GDI and GUI increased with worsening visual acuity, albeit the correlation was weak. Using
203	similar methods of distortion quantification, distortions were found to be higher in the amblyopic
204	population compared to non-amblyopic controls. (30, 35) Amblyopic observers experience chronic
205	distortion during development and may learn the spatial form of distorted optotypes. In contrast,
206	AMD patients have an acquired deficit later in life and visual distortion (metamorphopsia) arises at
207	the retinal level. Although research concerning the underlying basis of metamorphopsia in these
208	patient groups continues to be limited, it has been suggested that the visual processing stream in such
209	instances may be subject to top-down influences as a result of the slow progressing nature of the
210	aetiologies, potentially resulting in some degree of visual adaptation to the degraded image quality
211	and a resulting dissociation of perceived metamorphopsia from the visual acuity deficit. (31) Such
212	influences may also explain why we found a higher GUI (index of stability of the visual percept) that
213	correlated with certain clinical keratoconus indices.

214

215 In our sample, poorer BCVA was associated with greater maximum corneal curvature ( $\rho = 0.73$ ) and 216 TKC scores ( $\rho = 0.49$ ) but was not significantly correlated with CCT ( $\rho = -0.27$ ). Previous studies 217 have shown that visual acuity shows a variable degree of correlation with the corneal structural 218 measures and vision related quality of life in keratoconus. (9-11, 37) In comparison, contrast 219 sensitivity has been found to correlate with corneal irregularities (37), higher order aberrations (13), 220 and vision related quality of life (12). However, proper measurement of contrast sensitivity is time 221 consuming and traditional clinical tests of contrast sensitivity such as VisTech chart have limited 222 spatial frequencies for evaluation of moderate to advanced keratoconus. (15) Hence, the distortion 223 test used in the current study could provide an alternative or adjunctive visual measure for 224 keratoconus.

225

The visual distortion indices also correlated with commonly measured corneal structural parameters. Both GDI and GUI increased with higher corneal curvature, higher TKC and lower corneal thickness. The maximum corneal curvature ( $K_{max}$ ) and central corneal thickness better reflect the quality of life measures in keratoconus compared to visual acuity. (38, 39) Distortion measurement could therefore serve as a helpful bridge between clinical indicators and perceived quality of life that is quick and simple to administer.

232

233 In recent times home monitoring of different ocular conditions have been used (31, 40, 41) and these 234 have become even more important due to the COVID-19 pandemic, during which it has been 235 necessary in many instances to constrain in-person clinical interactions to essential care. Various 236 home-based applications implemented on the digital devices show good reliability compared to the 237 hospital-based tests for different ocular conditions. (40-44) As far as we are aware, there are no 238 systematic measures of distortion in keratoconus that could be utilised in this context. Proper 239 monitoring in keratoconus could ensure timely medical intervention such as collagen crosslinking but requires assessment by an eye care professional using specialist imaging equipment. A simple 240 241 monocular visual task such as that used in the current study could be easily transformed into a home-242 based tool. This also holds promise for individuals living with keratoconus in remote or rural areas 243 with limited specialist access. In future, we will develop a version of the distortion test for use on 244 personal or portable computing devices, to explore the use of the test as a home based tool for 245 keratoconus.

246

Some limitations can be identified for our study. Firstly, our paradigm provides information about distortion magnitude, but less about the individual's subjective percept, e.g. magnification, barrel distortion, etc. If clinically relevant, practitioners can store the square drawings to retain as a way of visually monitoring distortion over time. However, at present we are not able to offer a systematic method for detecting significant changes in the shape of the constructed square, which has the capacity to change significantly while yielding similar GDI and GUI measurements. This could be developed in future using image processing techniques or through methods such as subdivision into

- quadrant-based GDI and GUI measurements. Additionally, the value of a measurement tool to detect
- 255 progression of keratoconus remediation following treatment will depend on the repeatability of
- 256 distortion measurements, which is the focus of future work. Secondly, this was a cross-sectional
- study and we are unable to provide information about the extent to which treatments for keratoconus
- such as cross-linking may affect such measurements. As the correlation between BCVA and our
- 259 distortion measures was modest, we cannot be certain whether interventions to improve visual acuity
- 260 will impact GDI and GUI. As such, whether these distortion measures could be used to support
- 261 clinical decision-making about keratoconus interventions or as a treatment outcome measure should
- be a focus of future work.
- 263

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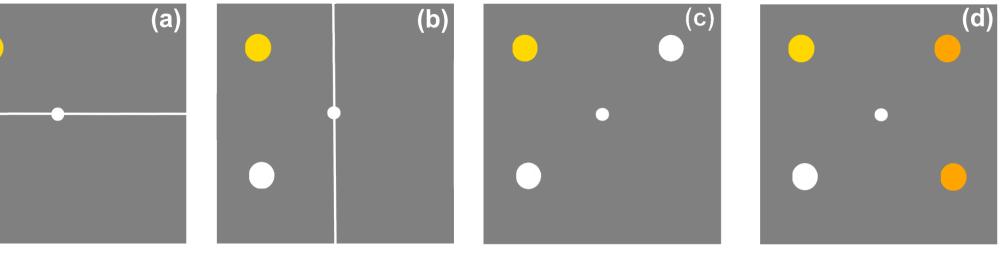
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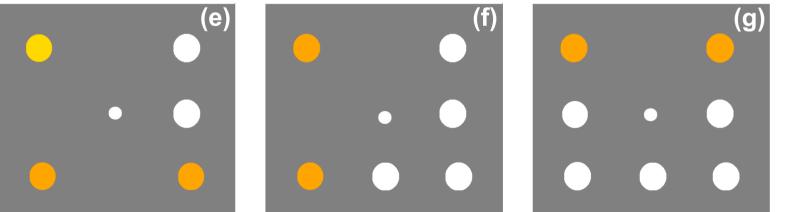
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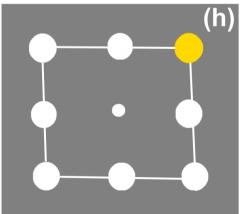
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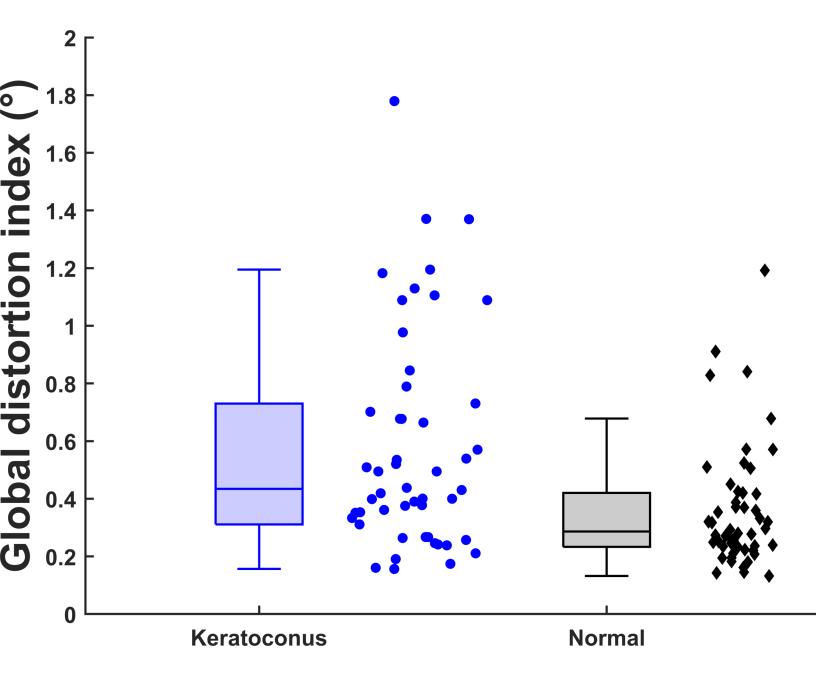
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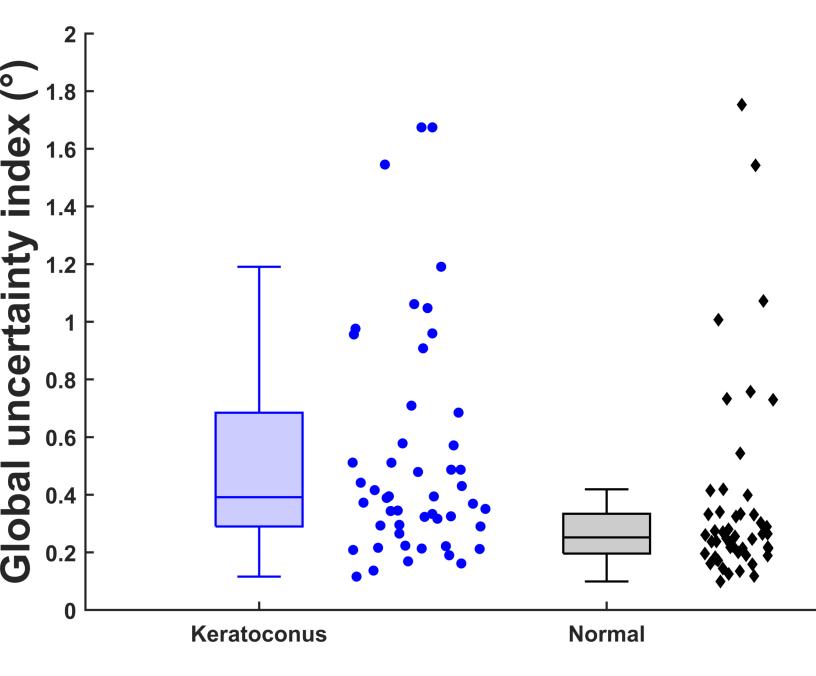
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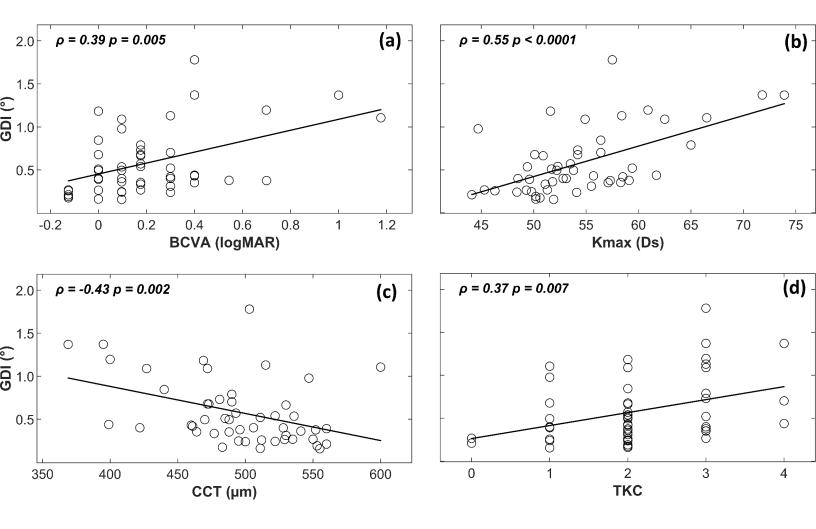


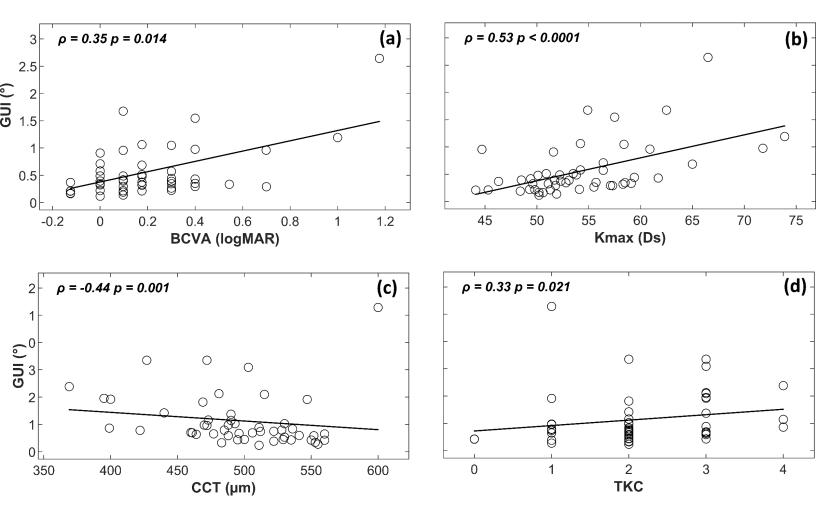












Clinical parameters	Keratoconus ( $n = 50$ eyes)
Best-corrected visual acuity, log MAR, mean (SD)	0.21 (0.27)
Refractive error (Sphere), diopter cylinder, mean (SD)	- 2.52 (2.85)
Refractive error (Cylindrical), diopter cylinder, mean (SD)	-3.45 (2.10)
Maximum corneal curvature, dioptre, mean (SD)	54.48 (6.09)
Mean corneal curvature, dioptre, mean (SD)	47.03 (3.96)
Central corneal thickness, micrometre (µm), mean (SD)	495.34 (47.50)

Control (n = 50 eyes)

-0.09 (0.06)

- 1.14 (1.61)

-0.77 (0.90)

45.66 (1.58)

44.51 (1.41)

554.36 (25.71)