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Optical quality of rotationally symmetrical contact lenses derived from their power profiles

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1 **Abstract**

2 Purpose: To present a methodology for evaluating the optical quality of rotationally
3 symmetrical contact lenses (CLs) from a sole power profile.

4 Methods: Simulated rotationally symmetrical power profiles corresponding to different
5 CLs designs (monofocal, two-zones center-near bifocal, and four-zones center-distance
6 bifocal) were used to calculate the wavefront error profile by means of numerical
7 integration. Then, each lens wavefront error profile was spun around the center to
8 obtain the lens wavefront error surface. From the surface, monochromatic optical
9 transfer functions (OTF), simulated images and the visual Strehl ratio based on the OTF
10 (VSOTF) were obtained for different distances and pupil sizes (3 and 5.5 mm) after
11 performing a through-focus.

12 Results: VSOTF variations, taking into account both vergence and pupil size, were
13 presented for the three CLs designs. The monofocal design showed excellent optical
14 quality only for far vision, whereas the bifocal designs exhibited good optical quality for
15 far and near vision. Modulation transfer function (MTF) from each lens design, pupil size,
16 and work distance and simulated images agreed with the previous results.

17 Conclusions: The methodology presented here allows for a rapid and thorough
18 assessment of the optical quality of rotationally symmetrical CLs by means of optical
19 quality metrics, with a special interest in simultaneous image contact lenses. This
20 methodology may be useful for choosing the most suitable lens for each subject's visual
21 demands.

22

23 **Keywords:** contact lens, simultaneous image contact lens, optical quality, power
24 profiles

25 Introduction

26 Simultaneous image contact lenses (CLs) are the most popular CLs for presbyopia
27 compensation [1,2]. These lenses are based on the principle of simultaneous vision [1],
28 where two or more images are formed simultaneously at the subject's retina. For this
29 principle to work, the visual system must **select** the best focused image and suppress the
30 rest.

31 Currently, there is a fair amount of different simultaneous image CLs designs
32 available in the market (e.g. center-near, center-distance designs) with different
33 addition powers [1,2] **and different number of zones or rings**, and thus knowing their
34 power distribution is essential. In the last years, several studies have evaluated the
35 power distribution of simultaneous image CLs based on their power profiles [3-7]. A
36 power profile shows how the refractive power provided by a lens varies with the radial
37 distance. Typically, the power profiles analysed are from rotationally symmetric CLs,
38 since in this case a sole power profile represents the refractive power distribution of the
39 whole lens. If a CL does not present rotational symmetry (e.g. toric CL, angular patterns),
40 then one power profile is not enough to know the refractive power distribution of the
41 whole lens.

42 Power profiles, when interpreted correctly, offer useful information about the
43 work distances that simultaneous image CLs can cover and about the effect of pupil size
44 upon the power distribution [5,7]. However, power profiles cannot offer a thorough
45 analysis regarding the optical quality of these lenses. For this reason, a methodology
46 based on the vergence maps described by Nam et al. [8,9] was proposed. This

47 methodology allows the assessment of the optical quality of rotationally symmetrical

48 simultaneous image CLs by calculating the lens wavefront from a sole power profile.

49

50 **Methods**

51 Contact lenses designs

52 Three simulated power profiles were considered in this study. All the power
53 profiles corresponded to CLs that had a nominal power of 0 D and a spherical aberration
54 of -0.075 D/mm². A negative value of spherical aberration is typically found in some CLs.
55 The first power profile simulated a monofocal CL, the second a two-zone center-near
56 [1,2] bifocal design with an addition power of 2 D, and the third a four-zone center-
57 distance [1,2] bifocal design, also with an addition power of 2 D. The power profiles of
58 these three CLs are shown in Figure 1.

59 Procedure

60 From now on it will be assumed that the power maps present radial symmetry,
61 hence it is enough to work with half of a power profile, also known as half-chord.

62 A wavefront vergence map (V), which is equivalent to a refractive power map,
63 can be derived from a wavefront error map (W) as follows [8–10]:

64

$$V(r,\theta) = n \frac{\delta W / \delta r}{r} \quad (1)$$

65

66 where r and θ are polar coordinates and n is the refractive index. The refractive
67 index is already taken into account in the measured vergence map. Assuming that, as
68 mentioned before, the refractive power map presents rotational symmetry, equation 1
69 transforms into

70

$$V(r) = \frac{\delta W / \delta r}{r} \quad (2)$$

71

72 From equation 2, the profile of the wavefront error map can be calculated by
73 integrating the profile along the radial direction, as:

74

$$W(r) = \int V(r)rdr \quad (3)$$

75

76 Since the power map was considered to have rotational symmetry, the resultant
77 wavefront error profile can be spun around the origin of the radial coordinates to obtain
78 the wavefront error map, which will be also rotationally symmetric.

79 Once the lens wavefront was obtained, a computational through-focus [11,12]
80 was performed by adding wavefronts with pure defocus to the lens wavefront. The
81 range of the through-focus was from 0 to 4 D of vergence, in steps of a fourth of 0.125
82 D. At each step of the through-focus, the optical transfer function (OTF) was obtained
83 for a wavelength of 550 nm. Then, the visual Strehl ratio based on the optical transfer
84 function (VSOTF) was calculated and used as a quality metric [13,14]. For each amount
85 of defocus, the VSOTF was computed using Fourier methods [13]. This metric was
86 chosen because it is known to correlate well with subjective measures of visual
87 performance [15]. This procedure was repeated for pupil diameters ranging from 0 to 6
88 mm, in 0.0625 mm steps.

89 A threshold for acceptable vision was set at VSOTF = 0.12, which has been used
90 previously [16,17]. This threshold corresponds to a 0.2 logMAR visual acuity [18] and it
91 can be considered as the limit where half of the people show difficulty in reading [19].
92 Therefore, values greater or equal than the mentioned threshold are considered to
93 provide acceptable vision. In addition, retinal images were calculated by convolving the
94 point spread function (PSF) of each design for far and near distances for pupil diameters
95 of 3 mm and 5.5 mm, with a chart composed of four letters that corresponded to a visual
96 acuity of 0.2 logMAR. The modulation transfer function (MTF) for the cases described
97 before was also calculated and shown. All the computations shown in this work were
98 performed using MATLAB (MathWorks, Inc., Natic, MA, USA).

99 Results

100 The VSOTF values for each design, with respect to the vergence and the pupil
101 diameter can be seen in Figure 2. The white solid curves demarcate the zones where the
102 VSOTF was equal or greater than 0.12. The upper panel corresponds to the VSOTF values
103 obtained for the monofocal design, which presents only optimal VSOTF values at one
104 vergence or working distance, in this case far. The peak got displaced to the right as the
105 pupil diameter increased as a consequence of the negative spherical aberration [20].
106 The mid panel shows the VSOTF map for the center-near design. It is evident that for
107 small pupils this design offered good optical quality only for near distances and the
108 optical quality increased again for far when the pupil became larger than 3 mm in
109 diameter. Lastly, the lower panel presents the VSOTF map for the center-distance
110 design. This design showed opposite behaviour than the center-near design, and also
111 slightly different optical quality distribution due to the complexity of the design.

112 Figure 3 shows how the optical quality **changed with respect to the vergence**.
113 These curves correspond to horizontal cuts in the maps showed in Figure 2 for a 3 mm
114 pupil size (left panel) and for a 5.5 mm pupil size (right panel). The solid gray curves
115 stand for the monofocal design, while the black solid and dashed curves stand for the
116 center-near and center-distance designs, respectively. The horizontal dotted black line
117 indicates the 0.12 threshold, thus the lenses provide acceptable vision at the vergences
118 where the curves are above this line.

119 Figure 4 shows the variation in the optical quality provided by each one of the
120 lenses when the pupil size changes. The left panel corresponds to the far distance,
121 whereas the right panel corresponds to the near distance. It should be noted that +0.25

122 D was the vergence selected for far vision, and -1.75 D the one selected for near vision,
123 because of the small displacement in the peaks introduced by the negative spherical
124 aberration [20], which was more noticeable at larger pupils.

125 From Figure 4, it can be seen how the monofocal design (gray solid curves)
126 provides only good optical quality for the far distance, and it does not vary vastly as the
127 pupil size increases. The center-near design (black solid curves) shows good optical
128 quality outcomes for near distance with smaller pupils. This design starts showing
129 acceptable values of optical quality for far distance when pupil size is larger than 3 mm.
130 The behaviour of the center-distance (black dashed curves) design is opposite to the
131 behaviour of the center-near design.

132 Figure 5 shows the MTF obtained for each design when the pupil
133 diameter is 3 mm (upper row) and 5.5 mm (lower row), for both far (left column), and
134 near distances (right column). The dotted black curves represent the diffraction-limited
135 MTF in each case.

136

137 Discussion

138 A methodology that allows for a rapid and thorough assessment of the optical
139 quality of rotationally symmetrical CLs, based just on a power profile, has been
140 presented. It can be particularly useful in optical quality evaluation of simultaneous
141 image CLs [1,2] since the effect of the pupil size on these elements is paramount [21].
142 This methodology presents a series of advantages with regards to the direct evaluation
143 of power profiles, since further information, other than power distribution, can be
144 extracted. It can show also how an object would be seen through one of these lenses
145 allowing for more representative comparisons between different designs. Another perk
146 is the rapid evaluation of the optical quality at different work distances and for different
147 pupil sizes, which is essential when compensating presbyopia [21].

148 As an example, Figure 6 shows simulated images of four letters that correspond
149 to a visual acuity of 0.2 logMAR as they were seen through the different designs
150 considered in this work, for both far and near distances, and for pupils of 3 mm and 5.5
151 mm. The monofocal design offers high quality vision for far whereas the bifocal designs
152 offer good quality for far and adequate for near vision, depending on the aperture size.

153 Regarding the definition of acceptable vision adopted here, it should be noted
154 that different thresholds could be selected for this purpose. First, it depends on the
155 quality metric used to present the results. There are a wide variety of metrics [13] based
156 on wavefront, PSF, OTF, or even based on the simulated images, like the cross-
157 correlation [22]. The use of the VSOTF was justified here because of its better correlation
158 with visual acuity than other metrics [18]. In addition, a 0.2 logMAR threshold was
159 chosen [19], but another one **could** be selected with proper justification. For example, a

160 threshold could be estimated by measuring subjective visual performance with different
161 simultaneous image CLs and correlate it with objective results derived from this
162 methodology.

163 One important limitation of this technique is the fact that the calculations were
164 performed for monochromatic light, thus not considering the effects of chromatic
165 aberration. Nevertheless, this can be partially solved by performing the same
166 calculations for different wavelengths, or adding polychromatic light to the
167 methodology [23]. Nevertheless, for adding the effect of polychromatic light to the
168 methodology, measurements of the power profiles of the lenses at different
169 wavelengths are required. Another limitation is that this methodology is valid only for
170 rotationally symmetric CLs. However, it is still useful since the majority of simultaneous
171 image CLs present rotational symmetry. Evaluating asymmetric CLs, such as toric CLs for
172 compensating astigmatism, requires a more complex technique that would allow for the
173 direct integration of the entire refractive power map.

174 This technique may be useful to evaluate the optical quality of CLs, in particular
175 simultaneous image CLs, by means of optical and visual quality metrics. Coupling the
176 wavefront of presbyopic eyes with the CL wavefront obtained as explained here could
177 be used for predicting the visual quality of the subject with a particular CL design. To do
178 so, a transfer of the lens wavefront from the lens plane to the pupil plane of the subject
179 should be performed. **Nevertheless**, a direct sum of wavefronts could work as an
180 approximation. This could help to choose the most suitable lens for each subject's visual
181 **needs. In addition, it could help** to study the effect of residual astigmatism and higher-
182 order aberrations **(especially spherical aberration)**, since it plays a major role in the

183 depth of focus of the eye [17,24,25], and on the visual quality of subjects wearing
184 simultaneous image CLs. Moreover, this methodology could be of use in designing new
185 simultaneous image CLs, aiming to improve patient satisfaction, by selecting the most
186 suitable addition, design and spherical aberration that provides the subject with the best
187 visual performance at the desired range of distances.

188

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251

252

253 **Figure legends**

254 **Figure 1.** Power profiles of the three CLs designs considered in this study. Upper panel
255 shows the power profile corresponding to the monofocal CL. Mid panel shows the power
256 profiles corresponding to the two-zone center-near design. Lower panel shows the
257 power profile corresponding to the four-zone center-distance design.

258 **Figure 2.** VSOTF maps with respect to the vergence (or work distance) and the pupil
259 diameter for the monofocal (upper panel), the center-near (mid panel) and the center-
260 distance (lower panel) designs. Black color indicates very poor optical quality, whereas
261 white color indicates very good optical quality. The white curves surround the areas of
262 acceptable vision ($VSOTF \geq 0.12$).

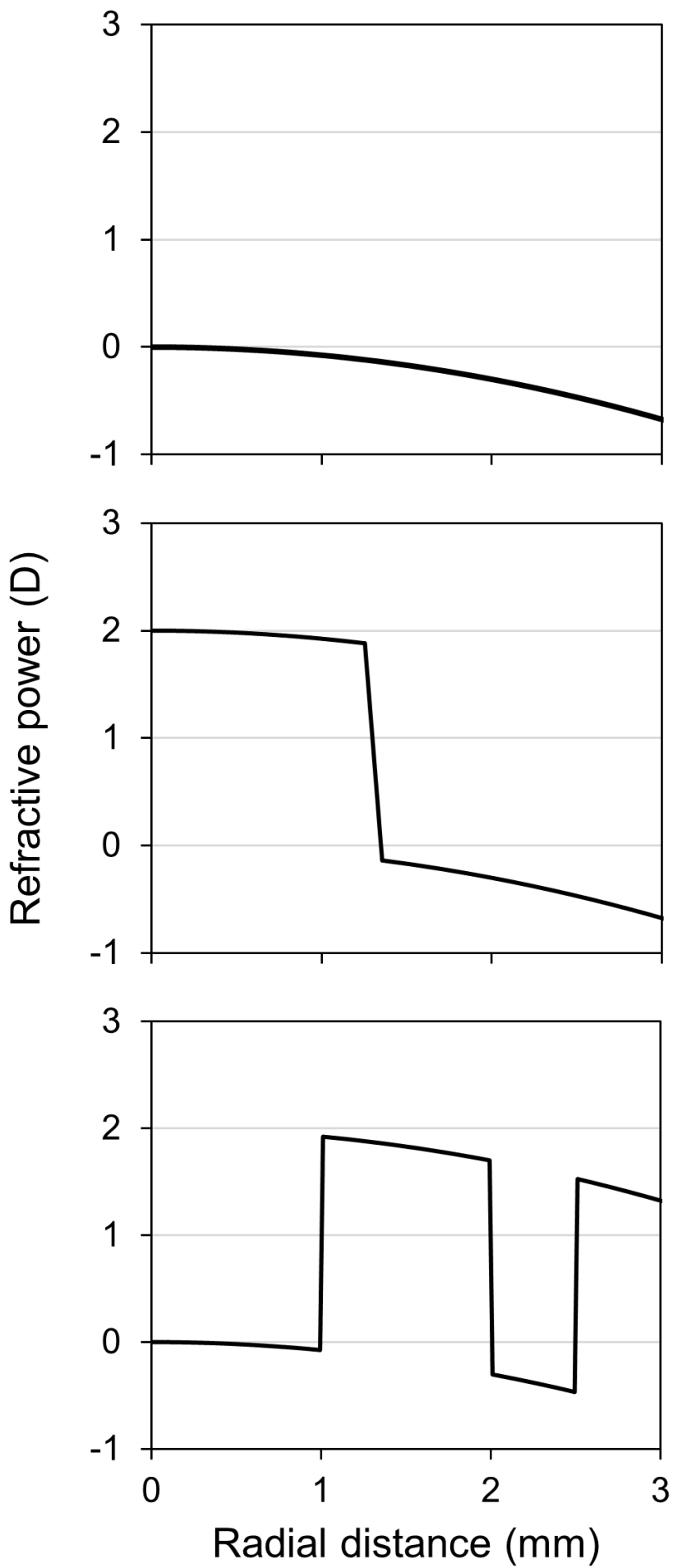
263 **Figure 3.** Variation of the optical quality (VSOTF) with respect to the vergence, or
264 working distance, obtained for the different designs when the pupil size is 3 mm (right
265 panel) and 5.5 mm (left panel). In both graphs the gray solid curves correspond to the
266 monofocal design, the black solid curves stand for the center-near design, and the black
267 dashed curves represent the center-far design. The dotted black line indicates the 0.12
268 threshold.

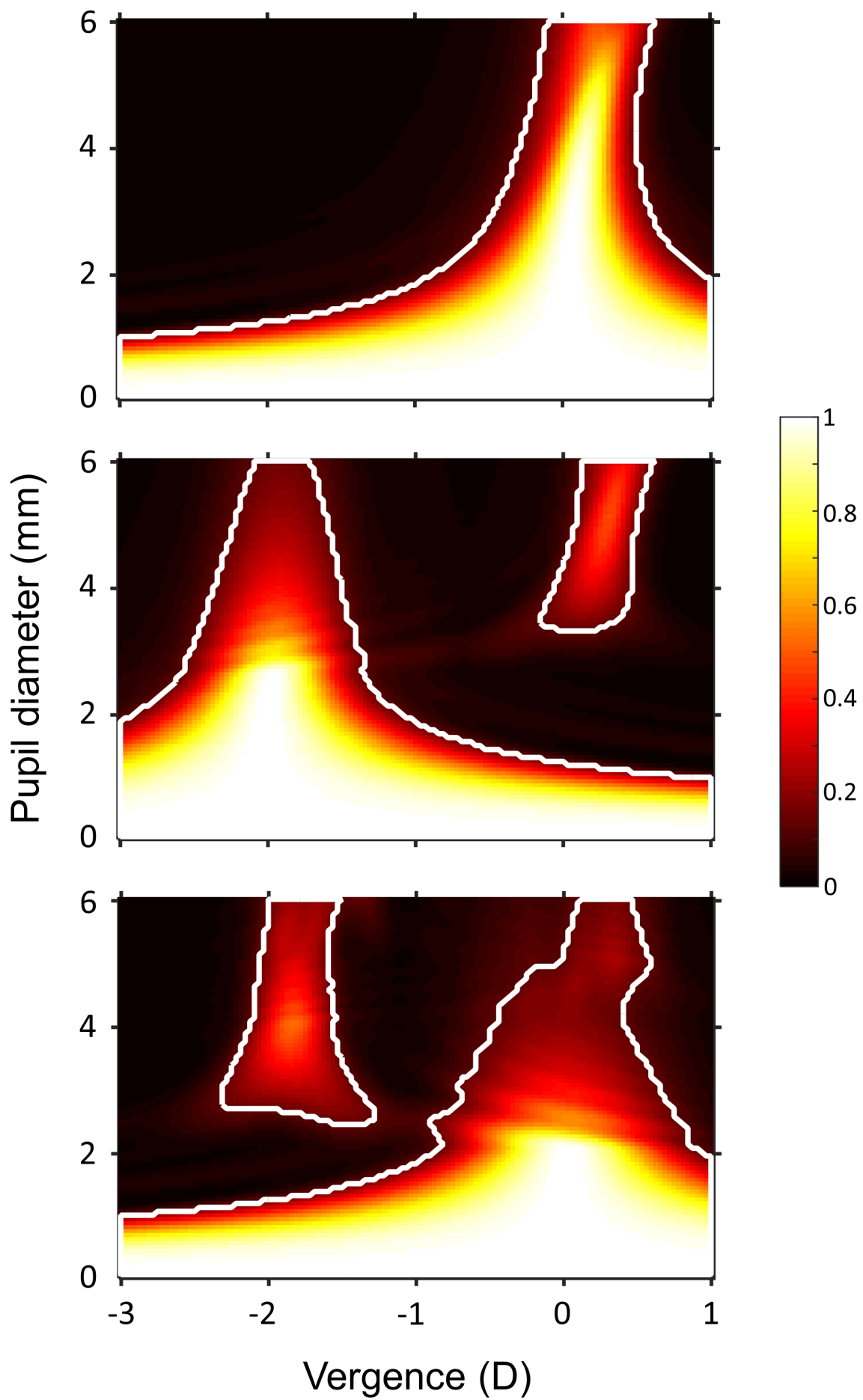
269 **Figure 4.** Variation of the optical quality (VSOTF) with respect to the pupil size, obtained
270 for the different designs for far distance (right panel) and near distance (left panel).
271 Other details as in Figure 3.

272 **Figure 5.** MTFs for the three different designs, plus the diffraction-limited MTF (black
273 dotted curves). The upper left panel shows the MTFs for far distance and a pupil
274 diameter of 3 mm; the upper left panel shows the same, but for near distance. Lower

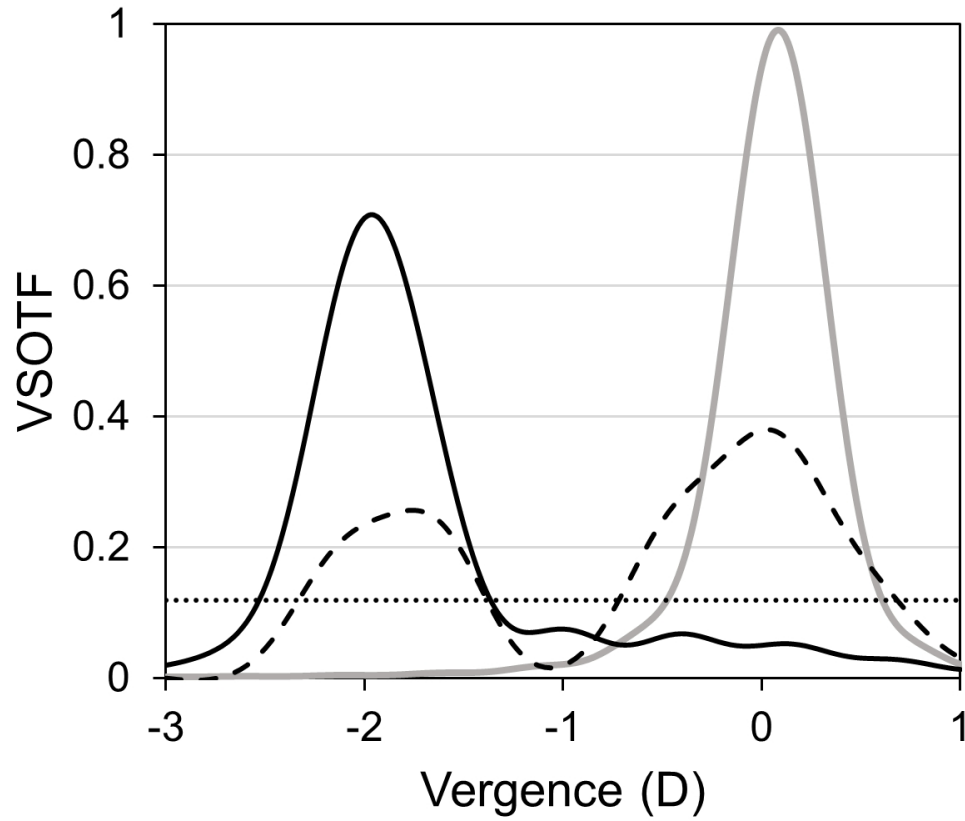
275 row represents the same, but for a pupil diameter of 5.5 mm. Other details as in Figure
276 3.

277 **Figure 6.** Simulation of images of a chart of letters corresponding to a 0.2 logMAR visual
278 acuity as seen through a pupil of 3 mm (upper block) and 5.5 mm (lower block), for each
279 design at both far and near distances.

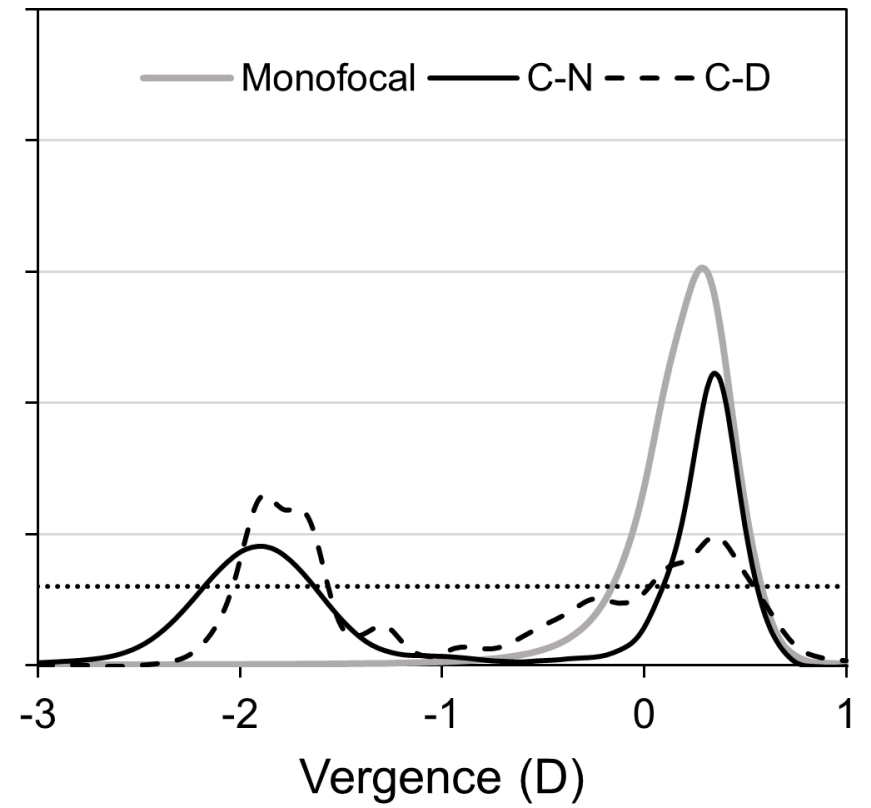




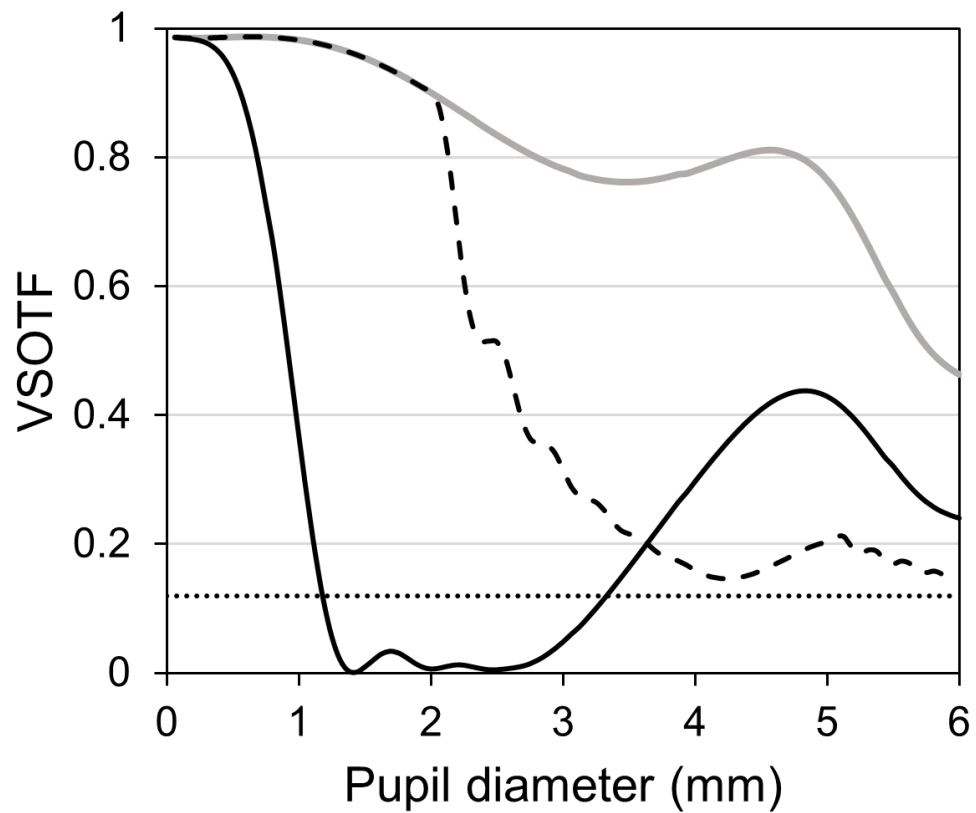
3 mm



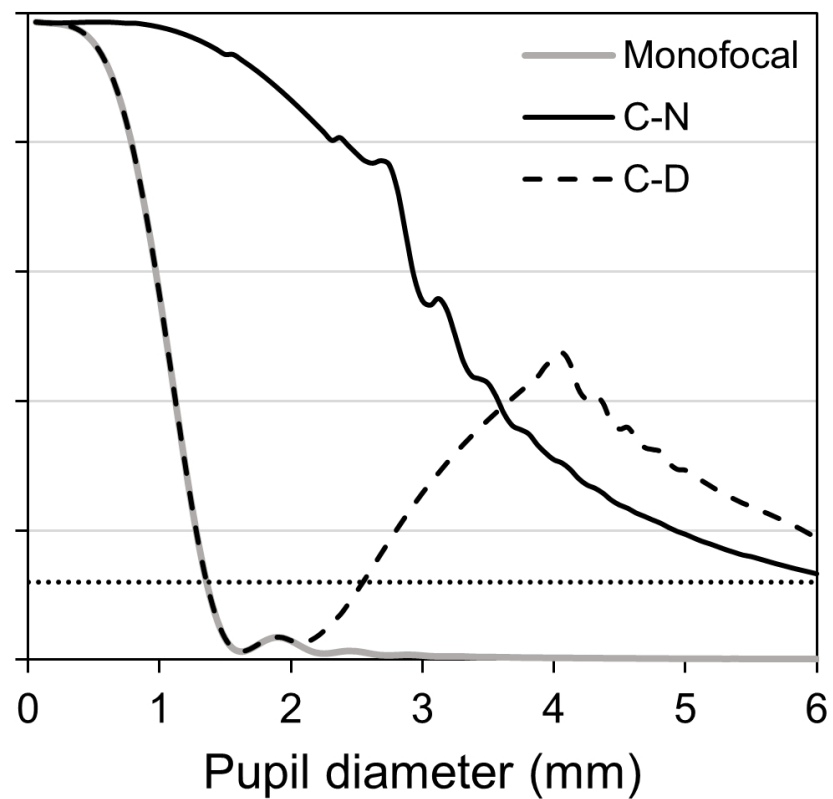
5.5 mm



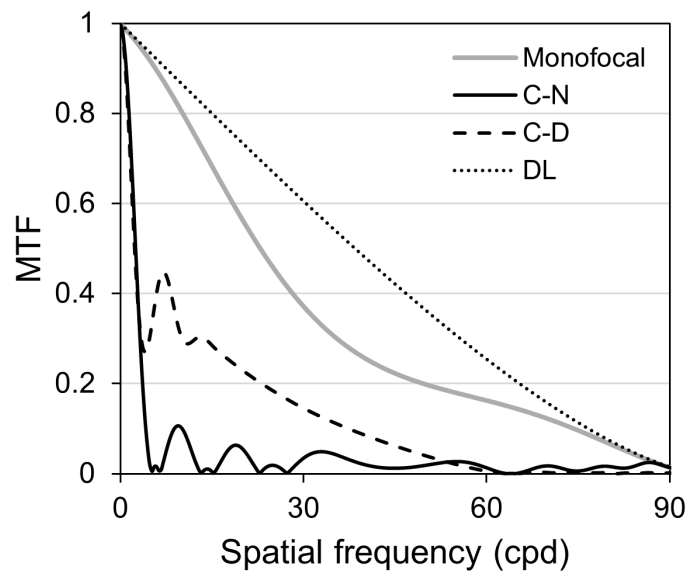
Far



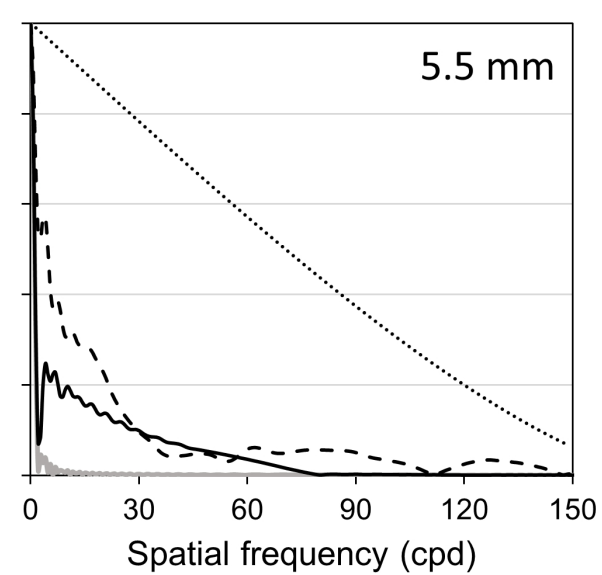
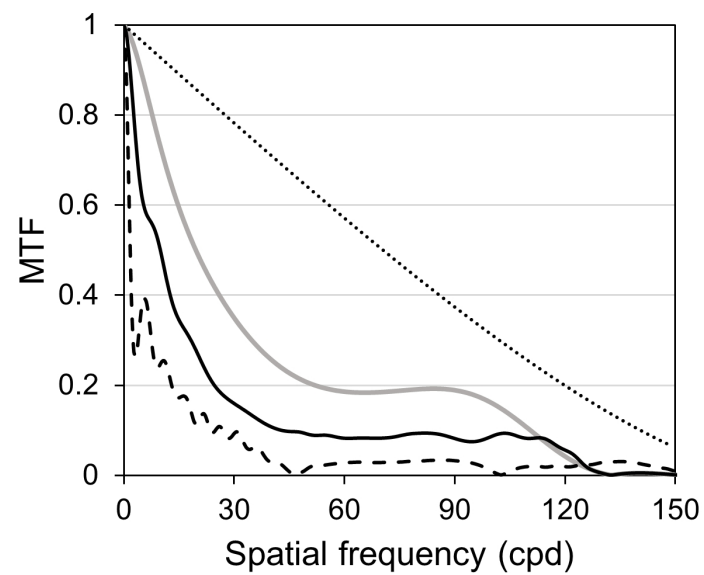
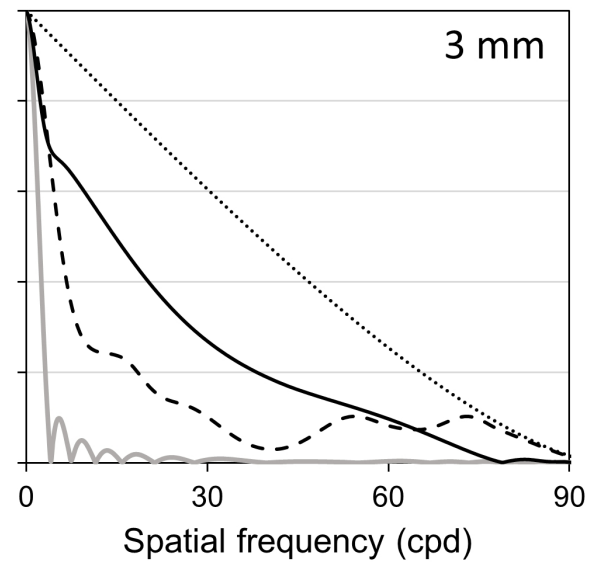
Near



Far



Near



Monofocal

Center-near
2 zones

Center-distance
4 zones

Far



3 mm

Near



Far



5.5 mm

Near



Manuscript Details

Manuscript number	<i>CLAE_2017_25</i>
Title	<i>Optical quality of rotationally symmetrical contact lenses derived from their power profiles</i>
Article type	<i>Short Communication</i>

Abstract

Purpose: To present a methodology for evaluating the optical quality of rotationally symmetrical contact lenses (CLs) from a sole power profile. **Methods:** Simulated rotationally symmetrical power profiles corresponding to different CLs designs (monofocal, two-zones center-near bifocal, and four-zones center-distance bifocal) were used to calculate the wavefront error profile by means of numerical integration. Then, each lens wavefront error profile was spun around the center to obtain the lens wavefront error surface. From the surface, monochromatic optical transfer functions (OTF), simulated images and the visual Strehl ratio based on the OTF (VSOTF) were obtained for different distances and pupil sizes (3 and 5.5 mm) after performing a through-focus. **Results:** VSOTF variations, taking into account both vergence and pupil size, were presented for the three CLs designs. The monofocal design showed excellent optical quality only for far vision, whereas the bifocal designs exhibited good optical quality for far and near vision. Modulation transfer function (MTF) from each lens design, pupil size, and work distance and simulated images agreed with the previous results. **Conclusions:** The methodology presented here allows for a rapid and thorough assessment of the optical quality of rotationally symmetrical CLs by means of optical quality metrics, with a special interest in simultaneous image contact lenses. This methodology may be useful for choosing the most suitable lens for each subject's visual demands.

Keywords	<i>contact lens; simultaneous image contact lens; optical quality; power profiles</i>
Taxonomy	<i>Contact Lenses, Presbyopia</i>
Corresponding Author	<i>Antonio J. Del Águila-Carrasco</i>
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Suggested reviewers	<i>David Madrid-Costa, Alberto Domínguez-Vicent</i>

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Antonio J. Del Águila-Carrasco
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Dear Editor,

Please find enclosed a manuscript entitled "*Optical quality of rotationally symmetrical contact lenses derived from their power profiles*" for consideration for publication in *Contact Lens and Anterior Eye* as a *Short Communication*. We confirm that this work is original and has not been published elsewhere nor is it currently under consideration for publication elsewhere. The manuscript assesses computationally the optical quality of different theoretical simultaneous image contact lenses, providing a great deal of information from just a simple power profile. To our knowledge, such a computational study has not been previously conducted and it may be useful for improving simultaneous image contact lens fitting.

Thank you for your consideration of this manuscript.

Sincerely yours,

Antonio J. Del Águila-Carrasco.

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37 distance. Typically, the power profiles analysed are from rotationally symmetric CLs,
38 since in this case a sole power profile represents the refractive power distribution of the
39 whole lens. If a CL does not present rotational symmetry (e.g. toric CL, angular patterns),
40 then one power profile is not enough to know the refractive power distribution of the
41 whole lens.

42 Power profiles, when interpreted correctly, offer useful information about the
43 work distances that simultaneous image CLs can cover and about the effect of pupil size
44 upon the power distribution [5,7]. However, power profiles cannot offer a thorough
45 analysis regarding the optical quality of these lenses. For this reason, a methodology
46 based on the vergence maps described by Nam et al. [8,9] was proposed. This

47 methodology allows the assessment of the optical quality of rotationally symmetrical

48 simultaneous image CLs by calculating the lens wavefront from a sole power profile.

49

50 **Methods**

51 Contact lenses designs

52 Three simulated power profiles were considered in this study. All the power
53 profiles corresponded to CLs that had a nominal power of 0 D and a spherical aberration
54 of -0.075 D/mm². The first power profile simulated a monofocal CL, the second a two-
55 zones center-near [1,2] bifocal design with an addition power of 2 D, and the third a
56 four-zones center-distance [1,2] bifocal design, also with an addition power of 2 D. The
57 power profiles of these three CLs are shown in Figure 1.

58 Procedure

59 From now on it will be assumed that the power maps present radial symmetry,
60 hence it is enough to work with half of a power profile, also known as half-chord.

61 A wavefront vergence map (V), which is equivalent to a refractive power map,
62 can be derived from a wavefront error map (W) as follows [8-10]:

63

$$V(r,\theta) = n \frac{\delta W / \delta r}{r} \quad (1)$$

64

65 where r and θ are polar coordinates and n is the refractive index. Assuming that
66 the refractive index is 1, and, as mentioned above, that the refractive power map
67 presents rotational symmetry, equation 1 transforms into:

68

$$V(r) = \frac{\delta W / \delta r}{r} \quad (2)$$

69

70 From equation 2, the profile of the wavefront error map can be calculated by
71 integrating the profile along the radial direction, as:

72

$$W(r) = \int V(r)rdr \quad (3)$$

73

74 Since the power map was considered to have rotational symmetry, the resultant
75 wavefront error profile can be spun around the origin of the radial coordinates to obtain
76 the wavefront error map, which will be also rotationally symmetric.

77 Once the lens wavefront was obtained, a computational through-focus was
78 performed by adding wavefronts with pure defocus to the lens wavefront. The range of
79 the through-focus was from 0 to 4 D of vergence, in steps of a fourth of 0.125 D. At each
80 step of the through-focus, the optical transfer function (OTF) was obtained for a
81 wavelength of 550 nm. Then, the visual Strehl ratio based on the optical transfer
82 function (VSOTF) was calculated and used as a quality metric [11,12]. For each amount
83 of defocus, the VSOTF was computed using Fourier methods [11]. This metric was
84 chosen because it is known to correlate well with subjective measures of visual
85 performance [13]. This procedure was repeated for pupil diameters ranging from 0 to 6
86 mm, in 0.0625 mm steps.

87 A threshold for acceptable vision was set at VSOTF = 0.12, which has been used
88 previously [14,15]. This threshold corresponds to a 0.2 logMAR VA [16] and it can be
89 considered as the limit where half of the people show difficulty in reading [17].
90 Therefore, values greater or equal than the mentioned threshold are considered to
91 provide acceptable vision. In addition, retinal images were calculated by convolving the
92 point spread function (PSF) of each design for far and near distances for pupil diameters
93 of 3 mm and 5.5 mm, with a chart composed of four letters that corresponded to a visual
94 acuity of 0.2 logMAR. The modulation transfer function (MTF) for the cases described
95 before was also calculated and shown.

96 **Results**

97 The VSOTF values for each design, with respect to the vergence and the pupil
98 diameter can be seen in Figure 2. The white solid curves demarcate the zones where the
99 VSOTF was equal or greater than 0.12. The upper panel corresponds to the VSOTF values
100 obtained for the monofocal design, which presents only optimal VSOTF values at one
101 vergence or working distance, in this case far. The peak got displaced to the right as the
102 pupil diameter increased as a consequence of the negative spherical aberration [18].
103 The mid panel shows the VSOTF map for the center-near design. It is evident that for
104 small pupils this design offered good optical quality only for near distances and the
105 optical quality increased again for far when the pupil became larger than 3 mm in
106 diameter. Lastly, the lower panel presents the VSOTF map for the center-distance
107 design. This design showed opposite behaviour than the center-near design, and also
108 slightly different optical quality distribution due to the complexity of the design.

109 Figure 3 shows how the optical quality varies in a through-focus. These curves
110 correspond to horizontal cuts in the maps showed in Figure 2 for a 3 mm pupil size (left
111 panel) and for a 5.5 mm pupil size (right panel). The solid gray curves stand for the
112 monofocal design, while the black solid and dashed curves stand for the center-near and
113 center-distance designs, respectively. The horizontal dotted black line indicates the 0.12
114 threshold, thus the lenses provide acceptable vision at the vergences where the curves
115 are above this line.

116 Figure 4 shows the variation in the optical quality provided by each one of the
117 lenses when the pupil size changes. The left panel corresponds to the far distance,
118 whereas the right panel corresponds to the near distance. It should be noted that +0.25

119 D was the vergence selected for far vision, and -1.75 D the one selected for near vision,
120 because of the small displacement in the peaks introduced by the negative spherical
121 aberration [18], which was more noticeable at larger pupils.

122 From Figure 4, it can be seen how the monofocal design (gray solid curves)
123 provides only good optical quality for the far distance, and it does not vary vastly as the
124 pupil size increases. The center-near design (black solid curves) shows good optical
125 quality outcomes for near distance with smaller pupils. This design starts showing
126 acceptable values of optical quality for far distance when pupil size is larger than 3 mm.
127 The behaviour of the center-distance (black dashed curves) design is opposite to the
128 behaviour of the center-near design.

129 Figure 5 shows the modulation transfer functions (MTF) obtained for each
130 design when the pupil diameter is 3 mm (upper row) and 5.5 mm (lower row), for both
131 far (left column), and near distances (right column). The dotted black curves represent
132 the diffraction-limited MTF in each case.

133

134 **Discussion**

135 A methodology that allows for a rapid and thorough assessment of the optical
136 quality of rotationally symmetrical CLs, based just on a power profile, has been
137 presented. It can be particularly useful in optical quality evaluation of simultaneous
138 image CLs [1,2] since the effect of the pupil size on these elements is paramount [19].
139 This methodology presents a series of advantages with regards to the direct evaluation
140 of power profiles, since further information, other than power distribution, can be
141 extracted. It can show also how an object would be seen through one of these lenses
142 allowing for more representative comparisons between different designs. Another perk
143 is the rapid evaluation of the optical quality at different work distances and for different
144 pupil sizes, which is essential when compensating presbyopia [19].

145 As an example, Figure 6 shows simulated images of four letters that correspond
146 to a visual acuity of 0.2 logMAR as they were seen through the different designs
147 considered in this work, for both far and near distances, and for pupils of 3 mm and 5.5
148 mm. The monofocal design offers high quality vision for far whereas the bifocal designs
149 offer good quality for far and adequate for near vision, depending on the aperture size.

150 Regarding the definition of acceptable vision adopted here, it should be noted
151 that different thresholds could be selected for this purpose. First, it depends on the
152 quality metric used to present the results. There are a wide variety of metrics [11] based
153 on wavefront, PSF, OTF, or even based on the simulated images, like the cross-
154 correlation [20]. The use of the VSOTF was justified here because of its good correlation
155 with visual acuity [16]. Also, a 0.2 logMAR threshold was chosen [17], but another one
156 can be selected with proper justification. For example, a threshold could be estimated

157 by measuring subjective visual performance with different simultaneous image CLs and
158 correlate it with objective results derived from this methodology.

159 One important limitation of this technique is the fact that the calculations were
160 performed for monochromatic light, thus not considering the effects of chromatic
161 aberration. Nevertheless, this can be partially solved by performing the same
162 calculations for different wavelengths, or adding polychromatic light to the
163 methodology [21]. Nevertheless, for adding the effect of polychromatic light to the
164 methodology, measurements of the power profiles of the lenses at different
165 wavelengths are required. Another limitation is that this methodology is valid only for
166 rotationally symmetric CLs. However, it is still useful since the majority of simultaneous
167 image CLs present rotational symmetry. Evaluating asymmetric CLs, such as toric CLs for
168 compensating astigmatism, requires a more complex technique that would allow for the
169 direct integration of the entire refractive power map.

170 This technique may be useful to evaluate the optical quality of CLs, in particular
171 simultaneous image CLs, by means of optical and visual quality metrics. Coupling the
172 wavefront of presbyopic eyes with the CL wavefront obtained as explained here could
173 be used for predicting the visual quality of the subject with a particular CL design. To do
174 so, a transfer of the lens wavefront from the lens plane to the pupil plane of the subject
175 should be performed, although a direct sum of wavefronts could work as an
176 approximation. This could help to choose the most suitable lens for each subject's visual
177 demands and to study the effect of residual astigmatism and of higher-order
178 aberrations, especially spherical aberration, since it plays a major role in the depth of
179 focus of the eye [15,22,23], and on the visual quality of subjects wearing simultaneous

180 image CLs. Moreover, this methodology could be of use in designing new simultaneous
181 image CLs, aiming to improve patient satisfaction, by selecting the most suitable
182 addition, design and spherical aberration that provides the subject with the best visual
183 performance at the desired range of distances.

184

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- 241
- 242

243 **Figure legends**

244 **Figure 1.** Power profiles of the three CLs designs considered in this study. Solid gray
245 curve stands for the monofocal design, black solid curve for the two-zones bifocal
246 center-near design, and black dashed curve corresponds to the four-zones bifocal
247 center-distance design.

248 **Figure 2.** VSOTF maps with respect to the vergence (or work distance) and the pupil
249 diameter for the monofocal (upper panel), the center-near (mid panel) and the center-
250 distance (lower panel) designs. Black color indicates very poor optical quality, whereas
251 white color indicates very good optical quality. The white curves surround the areas of
252 acceptable vision ($VSOTF \geq 0.12$).

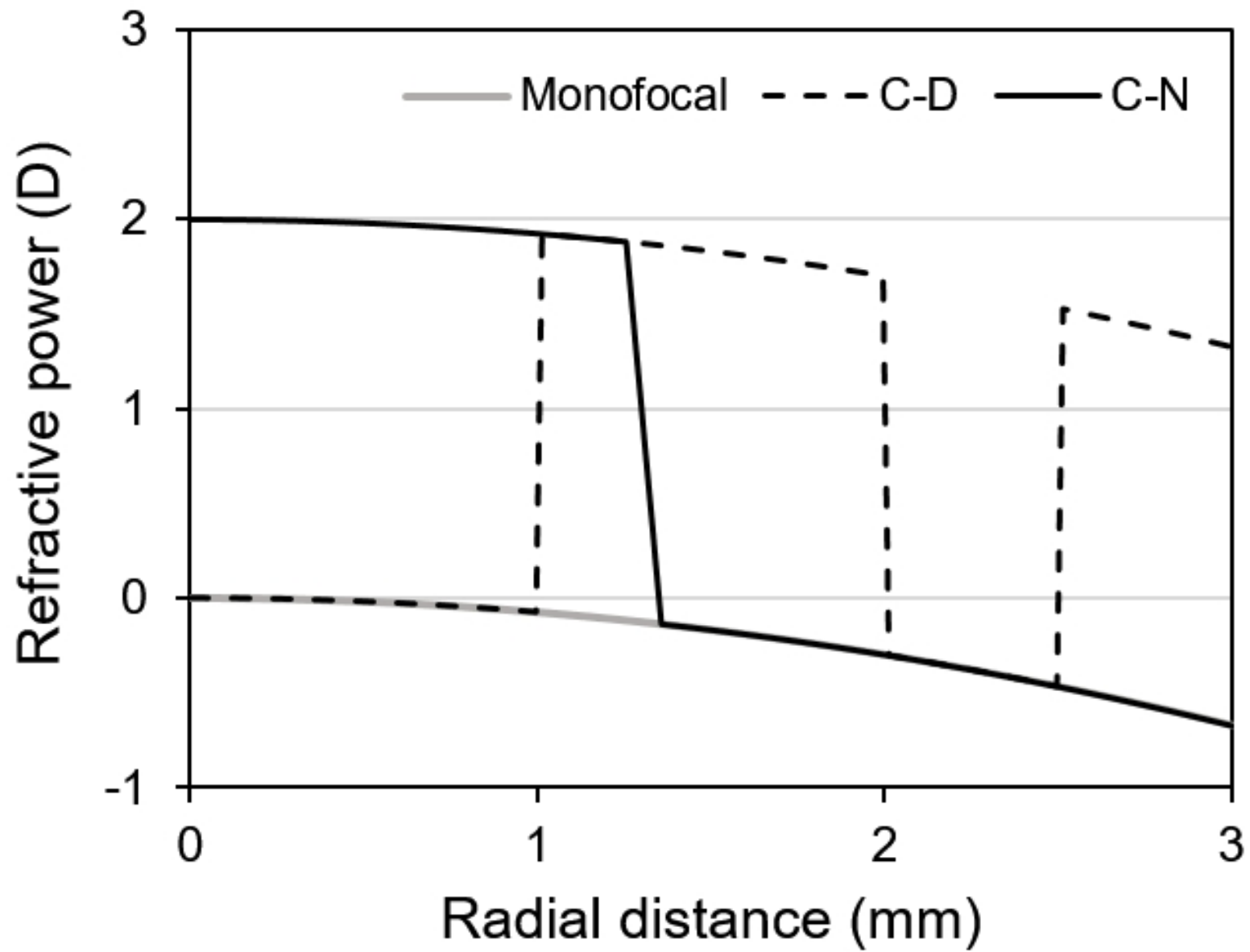
253 **Figure 3.** Variation of the optical quality (VSOTF) with respect to the vergence, or
254 working distance, obtained for the different designs when the pupil size is 3 mm (right
255 panel) and 5.5 mm (left panel). In both graphs the gray solid curves correspond to the
256 monofocal design, the black solid curves stand for the center-near design, and the black
257 dashed curves represent the center-far design. The dotted black line indicates the 0.12
258 threshold.

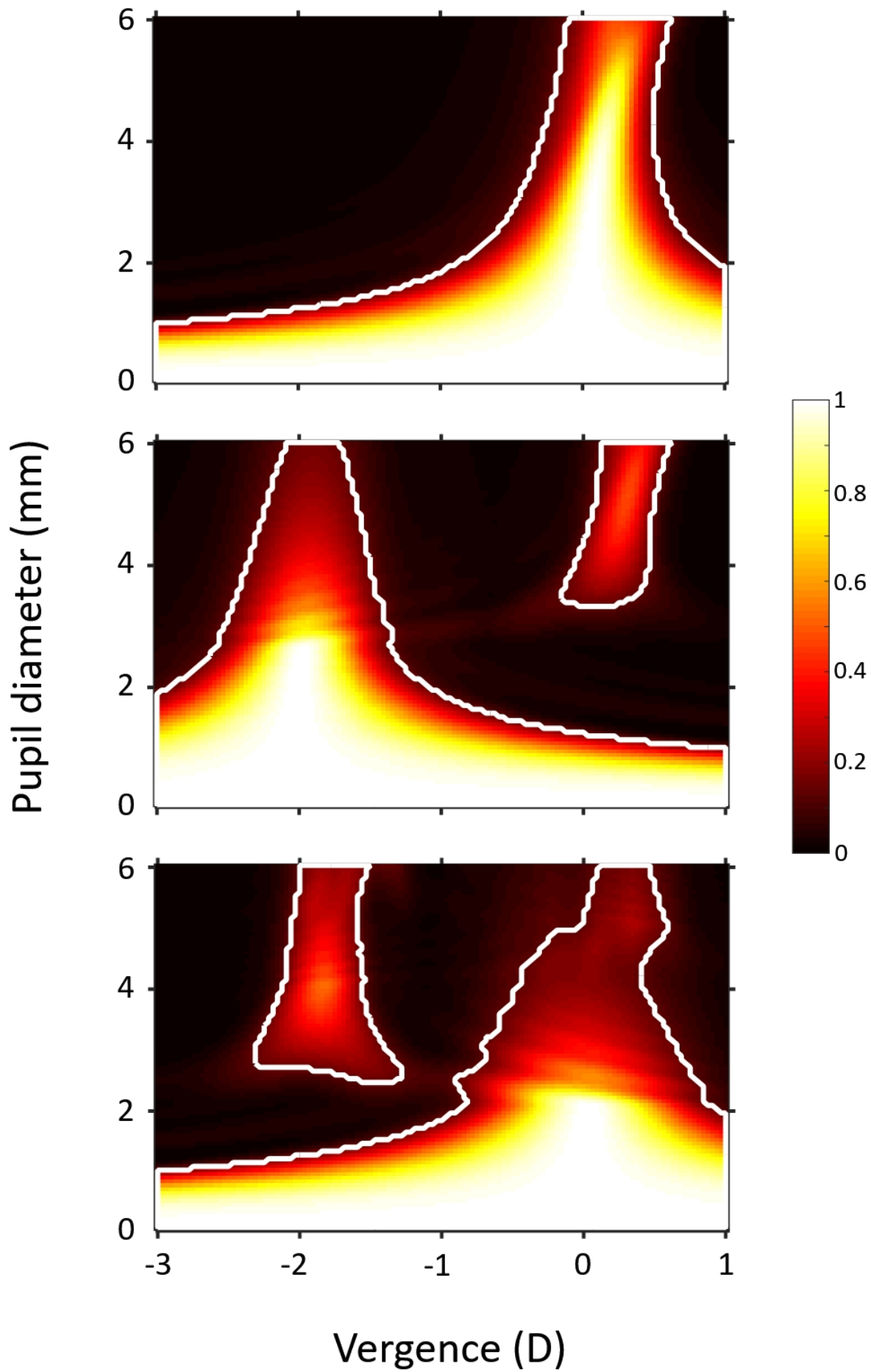
259 **Figure 4.** Variation of the optical quality (VSOTF) with respect to the pupil size, obtained
260 for the different designs for far distance (right panel) and near distance (left panel).
261 Other details as in Figure 3.

262 **Figure 5.** MTFs for the three different designs, plus the diffraction-limited MTF (black
263 dotted curves). The upper left panel shows the MTFs for far distance and a pupil
264 diameter of 3 mm; the upper left panel shows the same, but for near distance. Lower

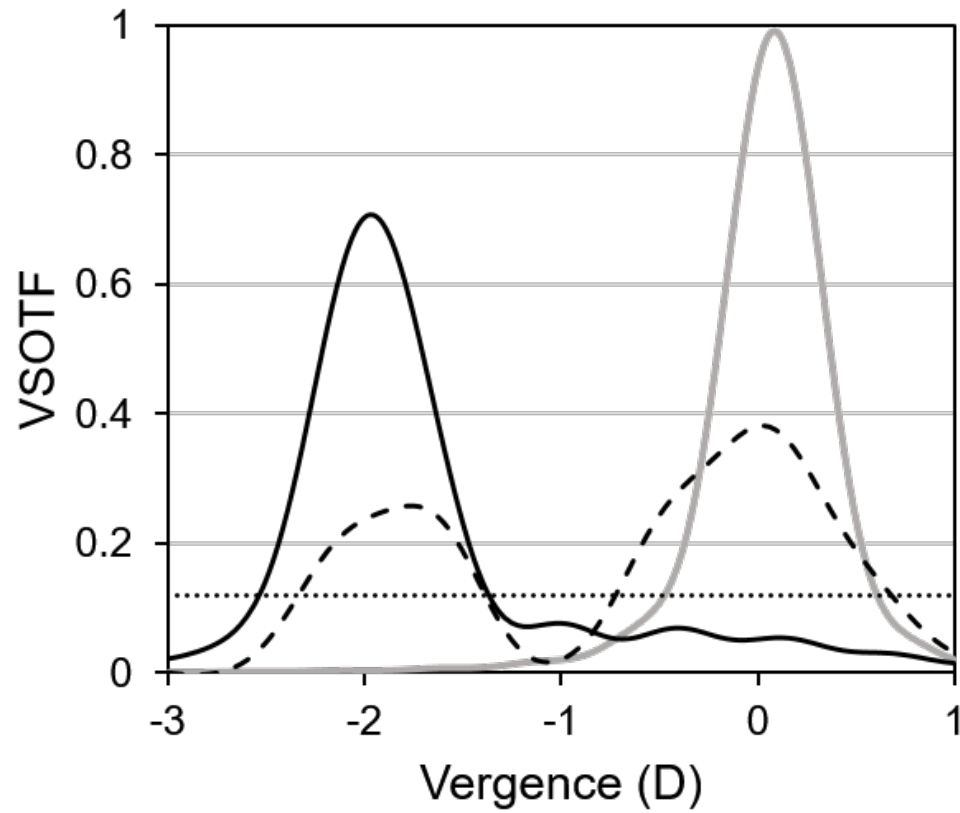
265 row represents the same, but for a pupil diameter of 5.5 mm. Other details as in Figure
266 3.

267 **Figure 6.** Simulation of images of a chart of letters corresponding to a 0.2 logMAR visual
268 acuity as seen through a pupil of 3 mm (upper block) and 5.5 mm (lower block), for each
269 design at both far and near distances.

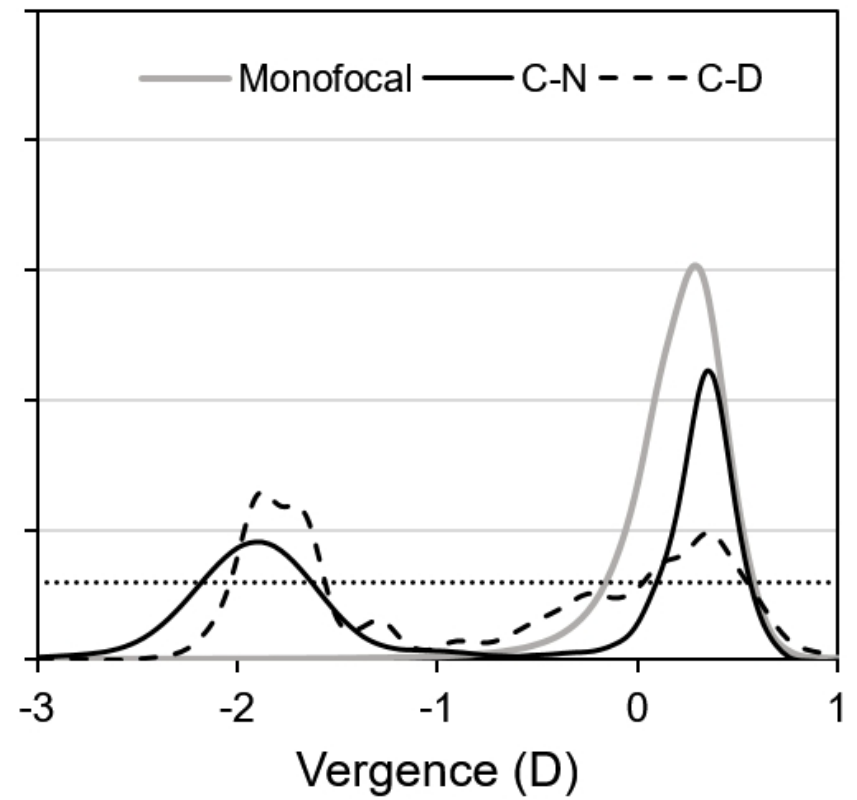




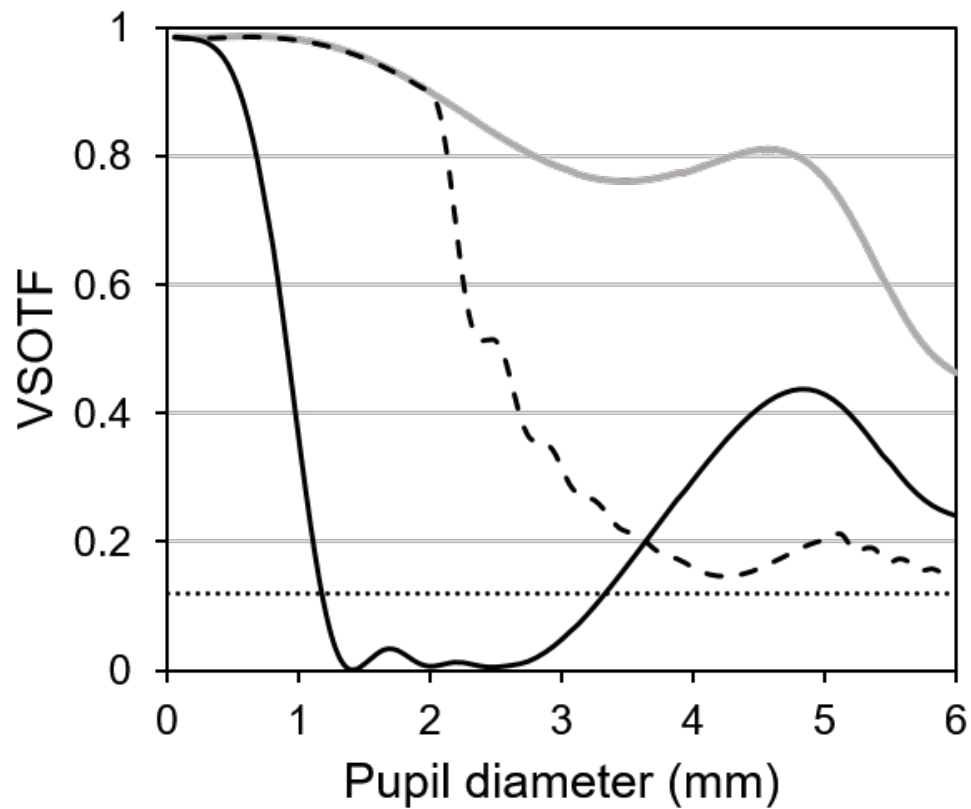
3 mm



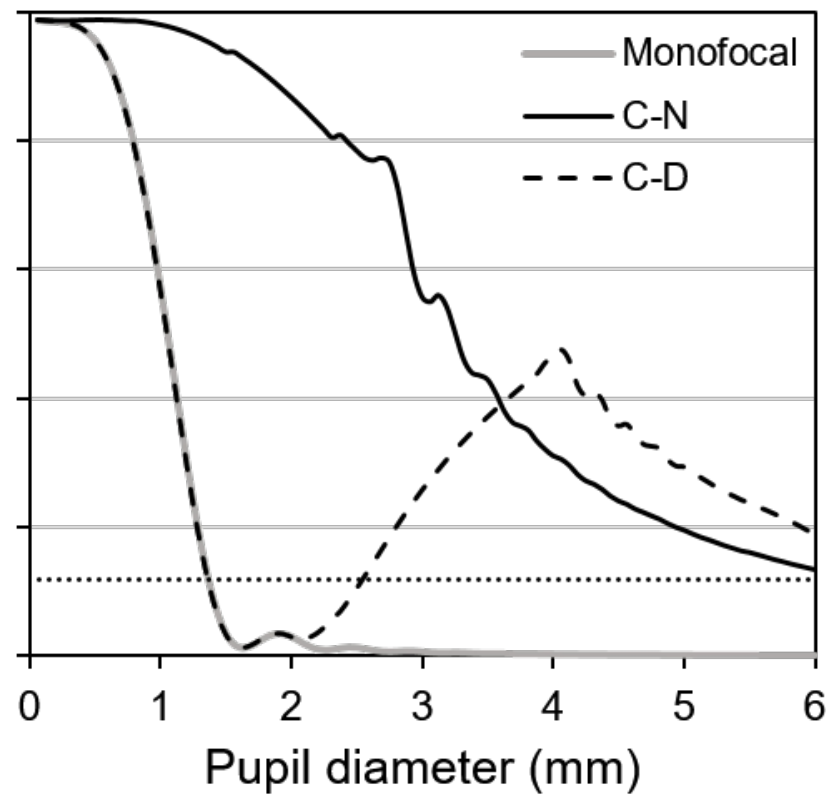
5.5 mm



Far

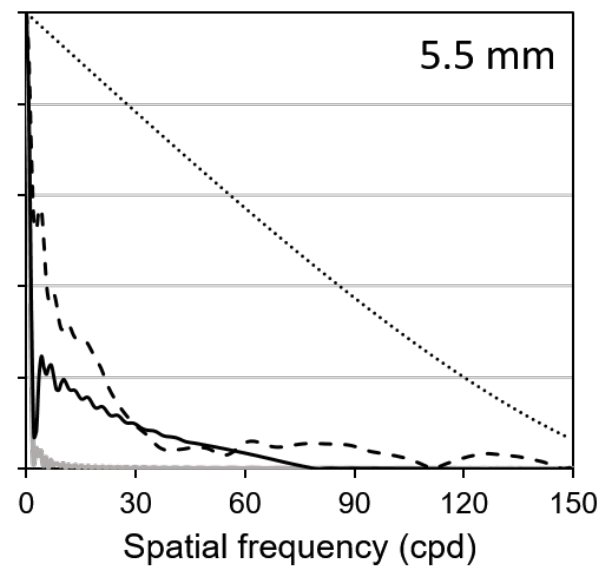
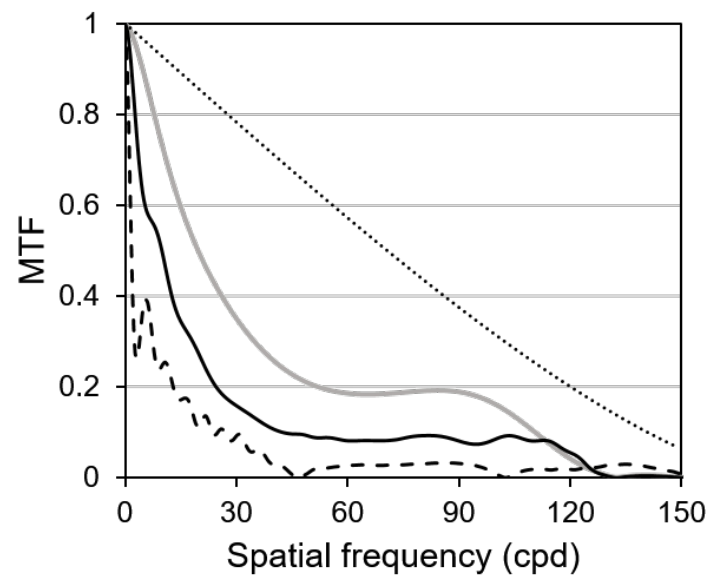
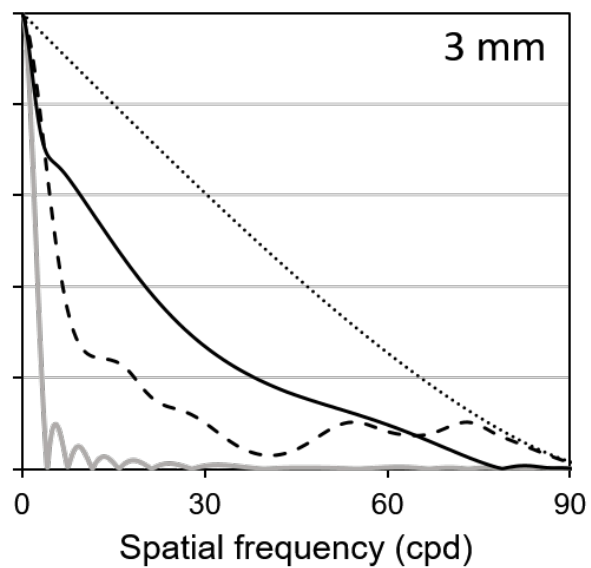
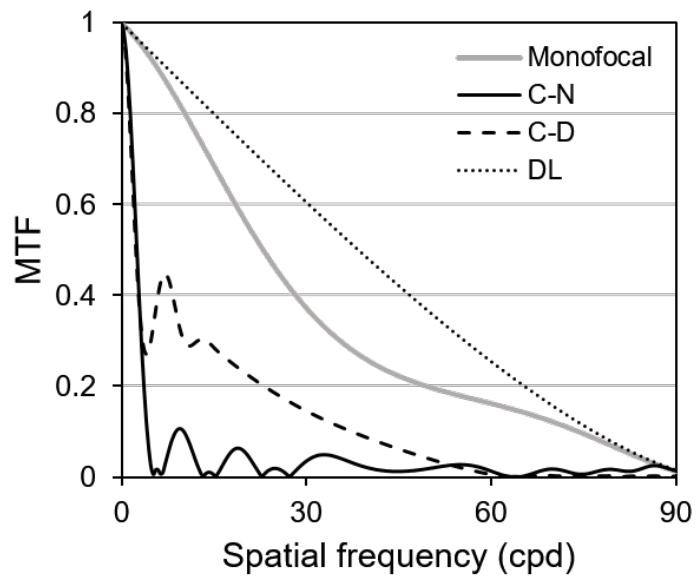


Near



Far

Near



Monofocal

Center-near
2 zones

Center-distance
4 zones

Far



3 mm

Near



Far



5.5 mm

Near



- A methodology for evaluating the optical quality of contact lenses is proposed.
- It only needs one power profile from the lens.
- Effect of pupil size and work distances can be rapidly assessed.

Optical quality of rotationally symmetrical contact lenses derived from their power profiles

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